

2D PHOTONIC CRYSTAL BASED BIOSENSOR USING RHOMBIC RING RESONATOR FOR GLUCOSE MONITORING

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Abstract

A 2D photonic crystal based biosensor using rhombic ring resonator is proposed and designed for monitoring the concentrations of glucose. The optical characteristics of rhombic ring resonator is analyzed and predicted by Finite Difference Time Domain method. A new structure of rhombic ring resonator is formed by utilizing bi-periodicity in the design of 2D silicon PC slab in hexagonal lattice with the size of 10 μm and 12 μm in X and Z direction, respectively. The sensing parameters are observed in the rhombic ring resonator which are completely depends on the refractive indices of the material used. Thereby the concentrations of glucose can be monitored. The determined sensing parameters such as resonant wavelength is about 1546 nm, quality factor is of 178.5, higher sensitivity of 1000nm/RIU and 100% of transmission efficiency is also achieved.

Keywords:

Photonic Crystal, Biosensor, Rhombic Ring Resonator, Sensitivity

1. INTRODUCTION

Generally, photonic crystals (PC) play a significant role for device miniaturization. PCs are periodic artificial materials, which cannot available naturally. The relative permittivity of the material is varied periodically with low and high dielectric value [1]. Photons propagate through structure or sometimes they do not propagate which depends on wavelength. The periodic structure do not allow certain range of wavelength which is termed as Photonic Band Gap (PBG). The propagation of electromagnetic waves inside the PBG region is zero. The photonic bandgap depends on three factors such as dielectric constant (Δ), lattice constant (a) and radius of the rod (r). By these factors waves are allowed to pass through the structure at particular wavelength or frequency. The two types of lattices in photonic crystal are cubic and hexagonal lattice. The photonic crystal is of three types, based on the geometry of structure such as 1D, 2D and 3D. Among these 2D photonic crystals are highly efficient as it provides an accurate bandgap calculation, better light confinement etc.

Biosensors are the devices which can be used to detect and analyze the samples with different characteristics [2]. They are more attractive due to its features like sensitivity, speed, accuracy etc. In optical sensing two approaches have been utilized namely, the impact of resonant wavelength shift scheme and intensity variation scheme. The shift of the resonant wavelength leads to higher sensitivity. Also based on the way in which samples to be tested, sensing mechanism is of two, such as homogeneous and heterogeneous or surface sensing. The heterogeneous sensing mechanism is employed here for monitoring the glucose samples.

The applications of photonic crystal based sensors are as follows, chemical sensing, force and strain sensing [3], refractive index and gas sensing [4], dengue virus detection [5], pressure sensing [6], aqueous environment [7] and biosensing (protein, avidins, BSA, DNA, blood constituents, glucose monitoring, etc.)

[8]. Photonic crystal based devices can also be designed for several applications such as filters [9], demultiplexers [10], switches [11], optical logic gates [12], polarization converters etc. [13].

In 2010, Hsiao and Lee have designed photonic crystal with nano ring resonator using hexagonal lattice of silicon rods for biochemical sensing where the biomolecules were trapped and the cumulative refractive index is varied. Then, the output resonant wavelength is shifted based on their refractive index change. In this they have achieved the quality factor as 3000 whereas sensitivity is about only 6nm/RIU [14]. In 2011, Pal et al. have designed PC with nano cavity coupled waveguides where the biosensing possibility is investigated by detecting human IgG molecules to achieve better sensitivity is of 64.5nm/RIU [15]. Olyaei et al. have proposed photonic crystal with nano cavity of hexagonal lattice using silicon rods. The biomaterials which are suspended in a liquid medium inside nano-cavities tends to effective refractive index changes which lead to the resonant wavelength shift in the output terminal. Here the quality factor is about 4793.6nm/RIU, then transmission efficiency is about only 75% and the sensitivity is about 65.7nm/RIU [16].

Dorfner et al. have also designed the photonic crystal with nano-cavity to analyze the concentrations of BSA. Drop filters have been added to improve sensitivity as 103 \pm 1nm/RIU [17] which is better than the sensitivity of 65.7nm/RIU. Further Kim et al. have reported the design of surface emitting photonic crystal with point band edge laser to investigate the performances of different refractive indices of liquids from 1.296-1.372 with span of 0.019. Thereby the sensitivity is getting improved as 135nm/RIU [18]. Moreover, in 2014, Najafgholinezhad and Olyaei have done an investigation on photonic crystal with microcavity resonator for analysis over the temperature dependency of water. There the achieved quality factor is of 15,000 but still sensitivity is of 141.67nm/RIU [19]. Thereby one thing can be noticed that sensitivity is inversely correlates with quality factor. Further, Dundar et al. have studied the concentrations of sugar water solution with nano cavity of hexagonal lattice. The achieved sensing parameters are as follows resonant wavelength is about 1475-1565nm, transmission efficiency is about 100% and sensitivity is of 280nm/RIU [20] better than the above.

Then, Kita et al. have demonstrated with nano lasers in hexagonal lattice for analyzing the performances of liquids with varying refractive indices from 1.00-1.37. The sensor is soaked into the liquids to obtain the sensitivity is about 350nm/RIU [21] and also resonant wavelength is in the range of 1570-1595nm. Here large amount of samples have needed to analyze the sensing parameters. Further, in 2016 to overcome above all criteria, M. S. Mohammed et al. have analyzed the PC with point defect in hexagonal lattice of GaN material to monitor the glucose concentrations. Here the resonant wavelength is about 1380-1440nm, average of quality factor is of 549.2, 60% of transmission

efficiency and over all higher sensitivity of 422nm/RIU is achieved in this literature [22].

Hence obviously, ultimate aim is to overcome and achieve higher order of sensing parameters. A 2D photonic crystal based biosensor is designed using rhombic ring resonator in hexagonal lattice for monitoring the glucose. The enhanced optical property material silicon is used here with the background of air which is better than GaN. The simulation result is obtained by Finite Difference Time Domain method [23]. Also higher order of sensing parameters can be achieved by this rhombic ring resonator such as resonant wavelength is in the range of 1540-1560nm, quality factor is of 178.6, 100% of transmission efficiency and sensitivity is of 1000nm/RIU. Hence the higher orders of sensing parameters are achieved in this paper which is greater than literatures reported before [14, 22, 15-21]. The rest of the paper is organized as follows, the proposed design is explained in section 2, simulation results and discussions are reported in section 3 and section 4 concludes the paper.

2. NUMERICAL ANALYSIS

The photonic crystals exhibited property called as Photonic Band Gap. The photonic band structure can be termed as an optical insulator. Since the transmission of electromagnetic waves in certain range of frequencies are prohibited, i.e., there is no propagation of light over some order of wavelengths. The light propagation can be manipulated by the defect mechanism. The line defect in the ring resonator acts as waveguide. Thereby, the sensitivity can be enhanced. In the ring resonator structure, the resonance and the output power can be altered as the refractive index of the sample gets varied. The photonic crystal functions as sensor can be proved by solving Maxwell’s electromagnetic equation [24].

$$\nabla \times \left(\frac{1}{\epsilon} \nabla \times H \right) = \left(\frac{\omega}{C} \right)^2 H \tag{1}$$

In Eq.(1), *H* is the magnetic field and *C* is the speed of light. Also, ϵ is the permittivity (dielectric function $\epsilon = \eta^2$ or $\eta = \sqrt{\epsilon}$ where η is the refractive index), ω is the frequency of resonance. It is observed that when the dielectric function changes the frequency also changes. From the Eq.(1) it is noticed that dielectric function ϵ is inversely proportional to frequency ω . The sensing performances of the structure can be analyzed by the Eq.(2) [25]:

$$L_{eff} = Q\lambda / (2\pi\eta) \tag{2}$$

In Eq.(2), *L_{eff}* is the effective interaction length, *Q* is the resonator quality factor, λ is the resonant wavelength, η is the refractive index of ring resonator.

3. PROPOSED DESIGN

3.1 PHOTONIC BAND GAP

The Fig.1 depicts the band diagram of hexagonal lattice without introducing any defects. The defects are nothing but breaking the periodicity by removing a row of rods (line defects) or single rod (point defect), changing the shape and size of the rods present in the structure and altering the structural parameters.

The band diagram has a PBG of TE mode and TM mode at different wavelength ranges which is listed in the Table.1. We have considered the wavelength range from 1125nm to 1725nm as it belongs to third window since it is highly efficient in the communication systems. The first TE PBG is accounted for further investigation, which is clearly pictured in blue colored region.

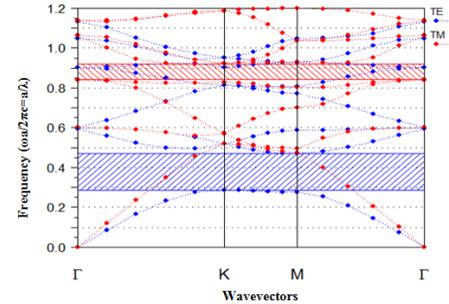


Fig.1. Band Diagram of Proposed Device

Table.1. Frequency and Wavelength from PBG

Types of PBG	Frequency (a/λ)	Wavelength (nm)
TE	0.480-0.313	1125-1725 nm
TM	0.954-0.865	566-624nm

The horizontal and vertical axes in the band diagram represent the wavevector and normalized frequency, respectively. The wavevector is calculated in the Brillouin zone, which is equal to the entire periodic structure. The normalized frequency of the PC structure is $\omega a / 2\pi c = a / \lambda$, where, ω is the angular frequency, *a* is the lattice constant, *c* is the velocity of light in free space and λ is the free space wavelength.

3.2 PC BASED BIOSENSOR

The Fig.2 depicts the designed photonic crystal based biosensor using rhombic ring resonator which consists of the hexagonal array of circular silicon rods placed in a background of air. In the hexagonal lattice, the total number of rods in X and Z direction are 21 and 21, respectively.

The proposed sensor consists of two optical waveguides namely bus waveguide and dropping waveguide. The bus waveguide acts as an input port placed at one end whereas dropping waveguide acts as an output port at another end. Both the waveguides can be designed by utilizing bi-periodicity.

Bi-periodicity is nothing but reducing the radii of rods in specific manner, such rods having radii of 50nm. Rhombic ring resonator is the heart of the proposed biosensor which is placed at the centre. It consists of two rings such as inner ring and outer ring rods. Both the radii of inner ring and outer ring rods are 105nm. Centre elliptical rod is of 150nm. The distance between the two rod is about 547nm, it is also called as lattice constant denoted by *a* and the dielectric constant of Si rod is 11.97 (refractive index = 3.46).

The Fig.3 shows 3D view of proposed sensor. The size of sensor is about 11.4µm×9.8µm. The simulation parameters of the sensor are listed in Table.2.

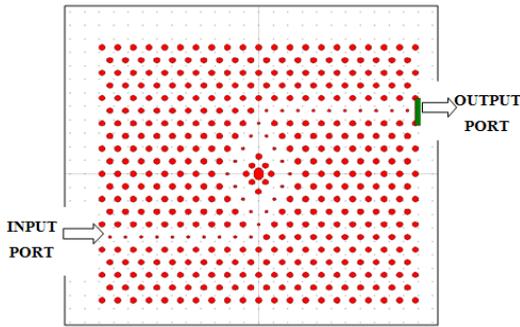


Fig.2. Schematic Representation of Proposed Biosensor

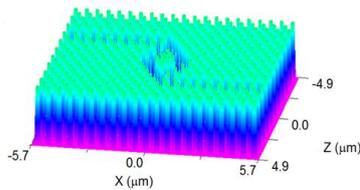


Fig.3. 3D View of Proposed Biosensor

Table.2. Simulation Parameters of Sensors

Design Parameters	Values
Configuration	Rod in air
Rod shape	Circular
Lattice structure	Hexagonal
Lattice constant	0.54 μm
Radius of rod	0.1 μm
Refractive index of rod	3.46
Dielectric constant of Si rod	11.97

When the light is propagating from bus waveguide (input port), through the rhombic ring resonator of sensor which is filled the sample, there is some molecular interactions due to the changes in the concentration of glucose sample results in variation of refractive indices of sample taken. Correspondingly, there is shift in the resonant wavelength along with the changes in the transmitted power. These can be observed at dropping waveguide (output port). Thereby better quality factor and sensitivity can be obtained. The sensitivity is defined as the resonance wavelength shift $\Delta\lambda$ per analyte refractive index change Δn [22].

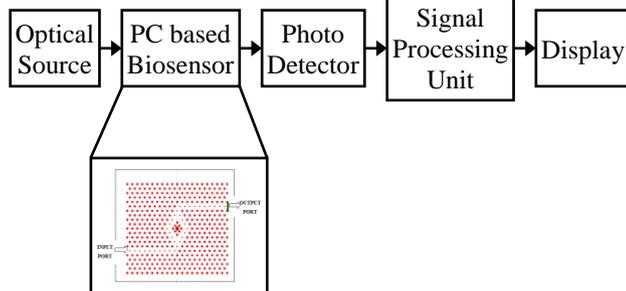


Fig.4. Schematic Structure of Glucose Sensor

The schematic representation of sensing mechanism is shown in Fig.4 consists of several components such as optical source, photonic crystal based biosensor, photo detector, signal processing unit and display. Optical source is the one by which the optical light is produced then reached in to the sensor where light is getting propagated through the glucose samples taken. Photo detector is used to convert electrical signal into optical signal. Then the output is processed in the signal processing unit. The processing includes filtering, modulation, demodulation, phase shifting, frequency conversion etc. Based on desired output the functions may be carried out in it. Finally output will be displayed in the display.

4. SIMULATION RESULTS AND DISCUSSION

When there is shift in refractive index of glucose sample then correspondingly there is shift in the resonance wavelength. According to that, there is shift in the level of glucose concentration. In such a way the sensor has to be designed. The normalized transmission spectrum of the sensor at 0 glucose level is shown in Fig.5. From that, obtained resonant wavelength, quality factor and transmitted efficiency is about 1545nm, 171.6 and 100%, respectively. The light signal is launched into the input port. The output signal power reaches the power monitor which is positioned at the output port is normalized by the input signal power.

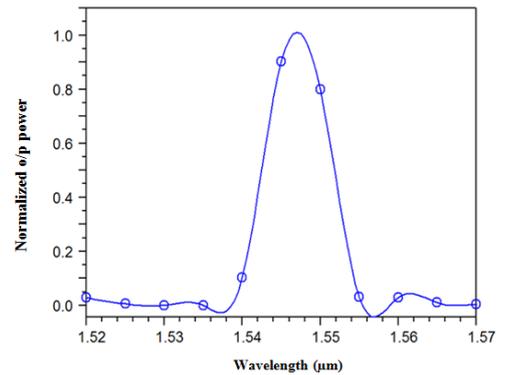
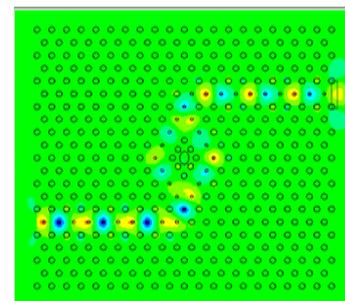


Fig.5. Normalized Transmission Spectrum of the Proposed Sensor at 0g/L

The electric field distribution of the proposed sensor at ON resonance and OFF resonance is representing in Fig.6(a) and Fig.6(b), respectively. It is clear that the signal couples in to the sensor at the resonance wavelength. The signals getting couples only at and above the resonance wavelength. This condition can be termed as ON resonance. When the signal is not able to couple below the resonant wavelength is about at 1300nm then that condition is called OFF resonance.



(a) $\lambda = 1560\text{nm}$

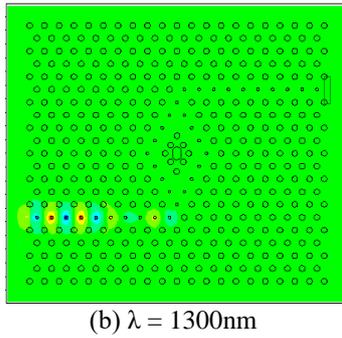


Fig.6. Schematic Representation of Field Distribution of sensor at (a) ON resonance (b) OFF resonance

The normalized output spectrum of proposed sensor is depicted in Fig.6. It is noticed that when the value of refractive index gets increase then resonance wavelengths also getting shifted accordingly.

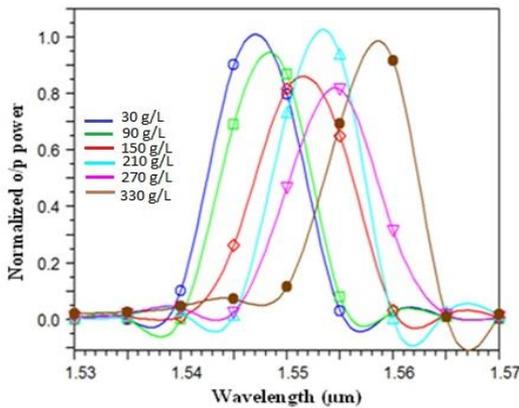


Fig.7. Normalized Transmission Spectrum of the Proposed Sensor

At 30g/L of glucose, the achieved resonant wavelength is about 1546nm, whereas other sensing parameters such as sensitivity is of 333.3nm/RIU, quality factor is about 171.7 and transmitted efficiency is of 100%. Also it is investigated that there is about 2.5nm of resonant wavelength shift is noticed for every increasing of 30g/L of glucose concentration. The refractive index, resonant wavelength, sensitivity, quality factor and transmission efficiency of the proposed biosensor at different glucose concentration is listed in Table.3. The maximum sensitivity, quality factor and transmission efficiency are 1000nm/RIU, 178 and 100%, respectively.

Table.3. Refractive Index, Resonant Wavelength, Sensitivity, Quality Factor and Transmission Efficiency of the Sensor at Different Glucose Concentration

Glucose Concentration (g/L)	Refractive Index	Resonant Wavelength (µm)	Sensitivity (nm/RIU)	Quality Factor	Transmission Efficiency (%)
30	2.460	1.546	333.3	171.7	100
90	2.466	1.548	666.6	110.5	80
150	2.472	1.551	1000	155.1	80
210	2.478	1.553	666.6	178.5	100
270	2.484	1.555	666.6	153.9	80
330	2.490	1.558	1000	173.1	95

5. CONCLUSION

The two dimensional photonic crystal based biosensor is designed and its sensing characteristics are analyzed. The sensor is designed using two dimensional photonic crystals with the hexagonal lattice of circular silicon rods surrounded by air. The sensor is designed in the wavelength range 1540nm to 1560nm. The resonance wavelength, sensitivity, Q factor and output power of the sensor are 1546nm, 1000nm/RIU, 178.5 and 100% respectively. The designed sensor is highly sensitive to refractive index. By knowing the refractive index value, the glucose concentration is obtained. The low level of urea excretion by kidney is indicator of kidney related diseases and the high level of urea excretion is due to higher protein intake and breakdown. So maintaining the glucose level in our body is really an important thing. Hence the sensor is designed in such a way to obtain the higher sensitive output.

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